



# FINITE ELEMENT MODELING AND ANALYSIS OF THE HUMAN SPINE

Presenter:

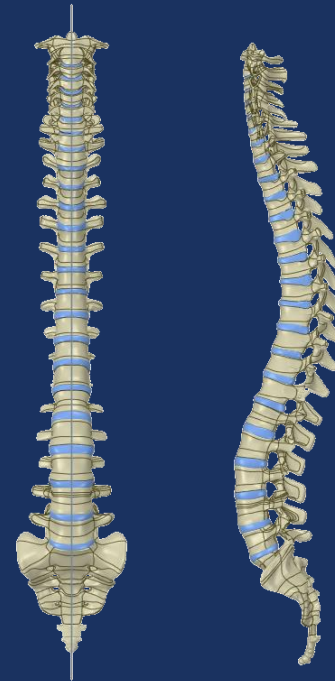
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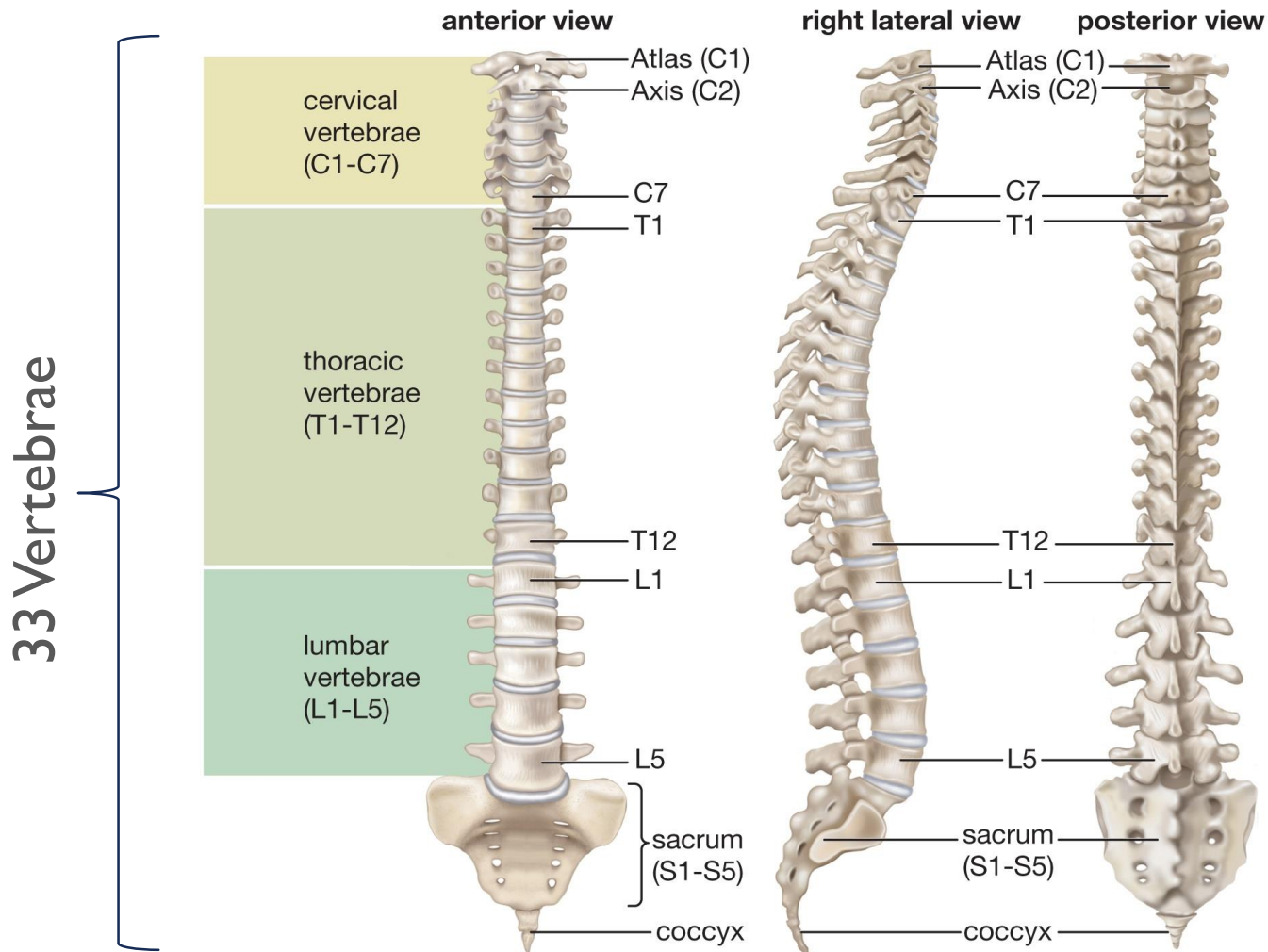
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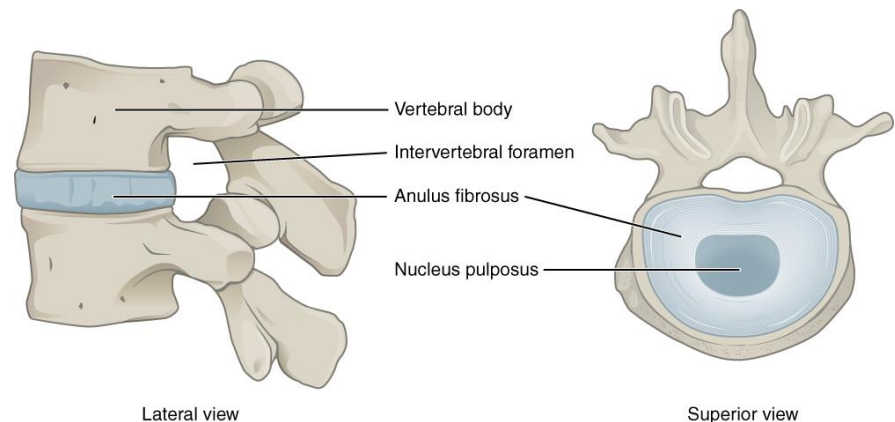
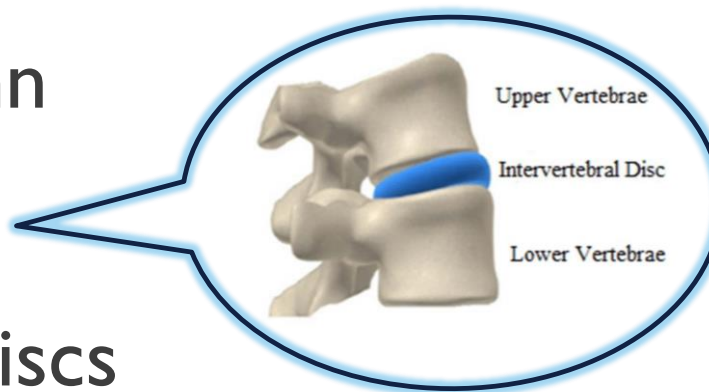
# STRUCTURE OF THE SPINE



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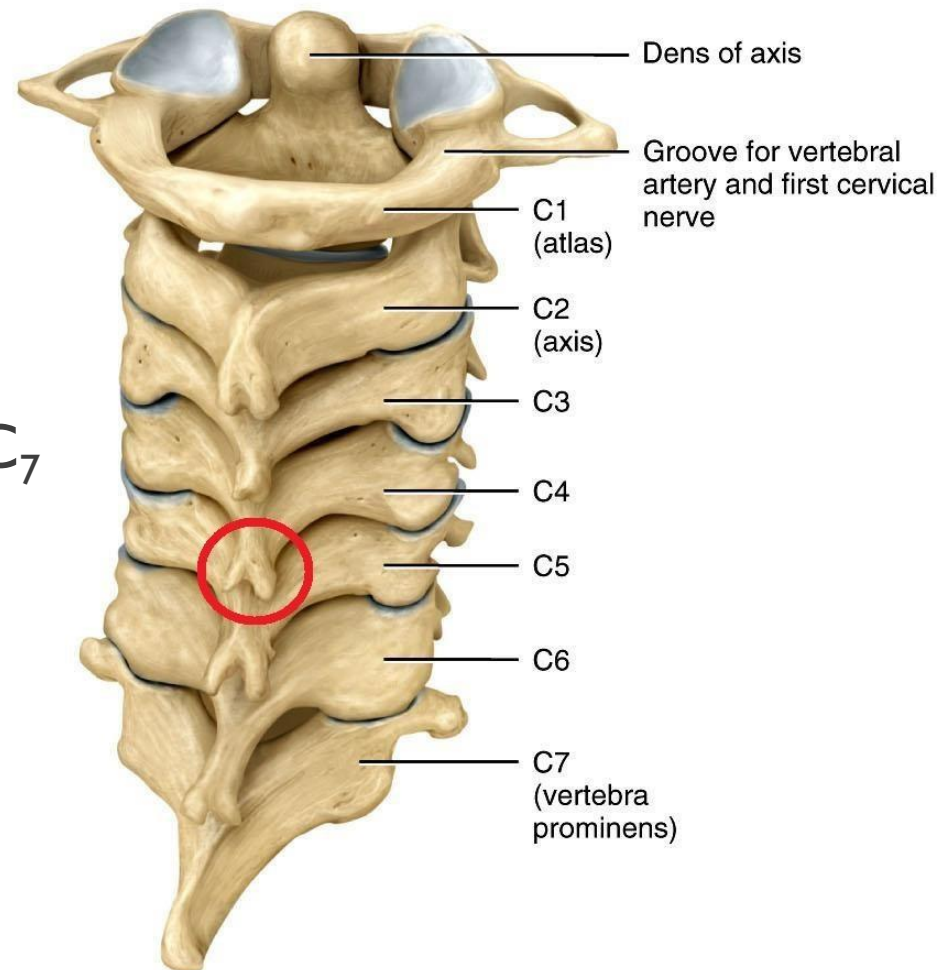
- Vertebral Column
- Motion Segment
- Intervertebral Discs
  - Annulus Fibrosus
  - Nucleus Pulposus



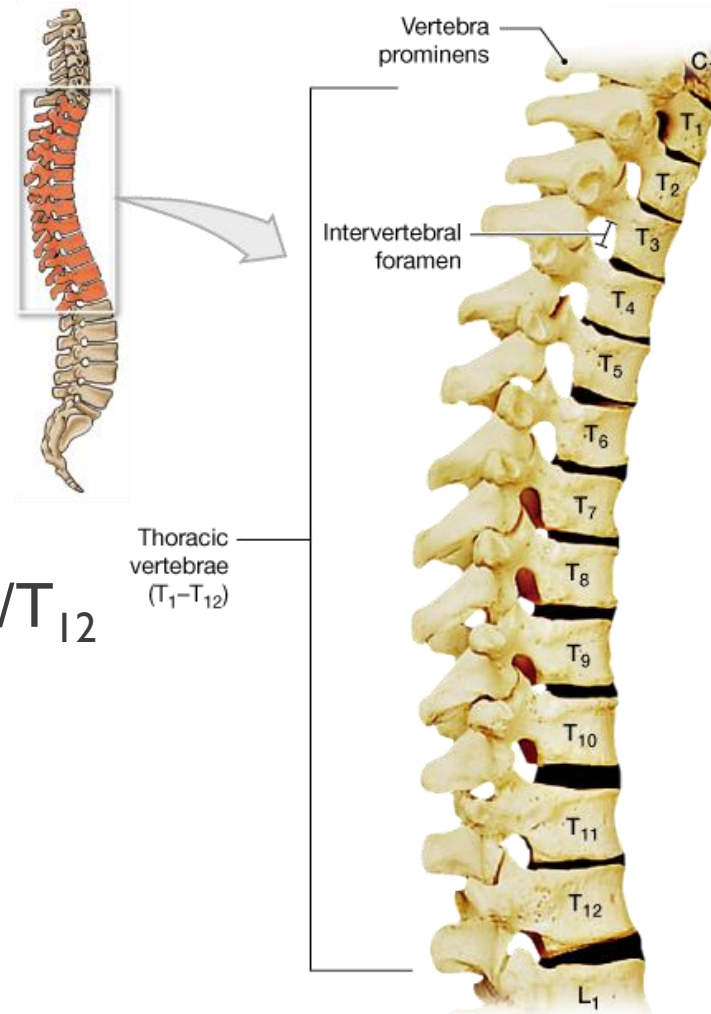
# CERVICAL VERTEBRAE



- Typical C<sub>3</sub>-C<sub>4</sub>-C<sub>5</sub>-C<sub>6</sub>
- Atypical vertebral C<sub>1</sub>/C<sub>2</sub> - C<sub>7</sub>



# THORACIC VERTEBRAE

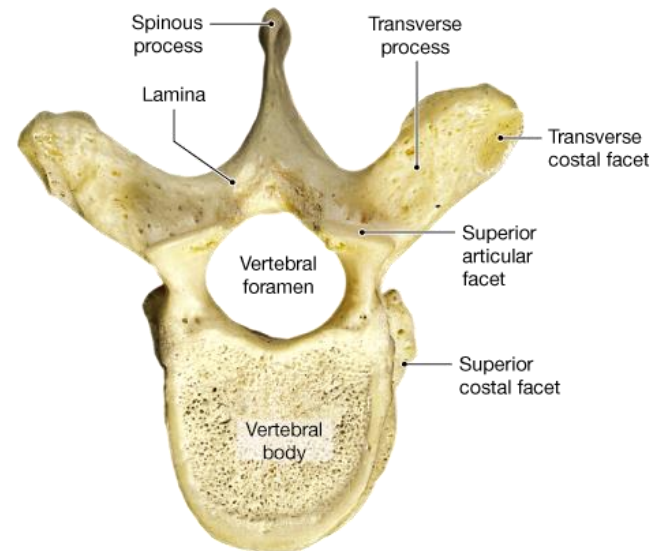


- Typical vertebrae T<sub>2</sub>-T<sub>9</sub>
- Atypical vertebrae T<sub>1</sub>/T<sub>10</sub>/T<sub>11</sub>/T<sub>12</sub>

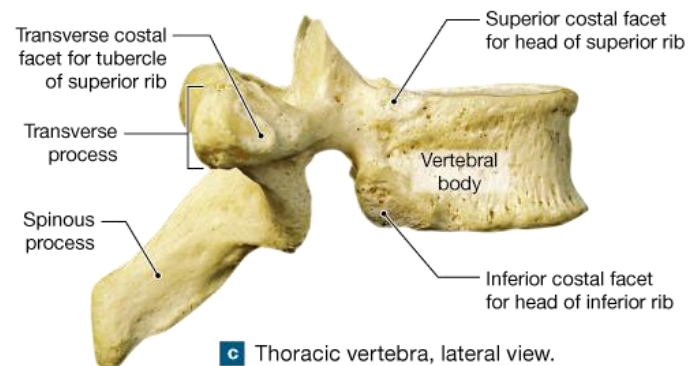
# THORACIC VERTEBRAE



- 1 spinous process
- 2 transverse process
- 2 superior facet
- 2 inferior facet



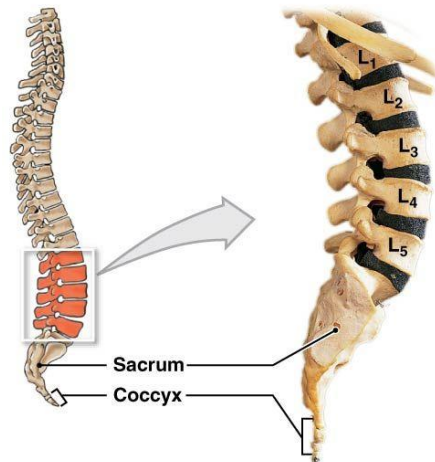
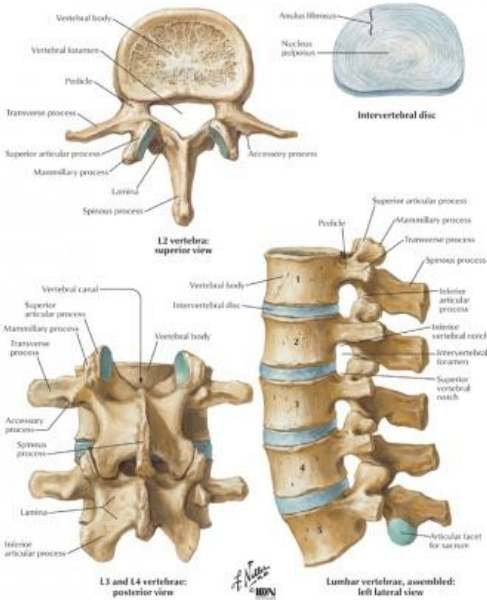
**b** Thoracic vertebra, superior view.



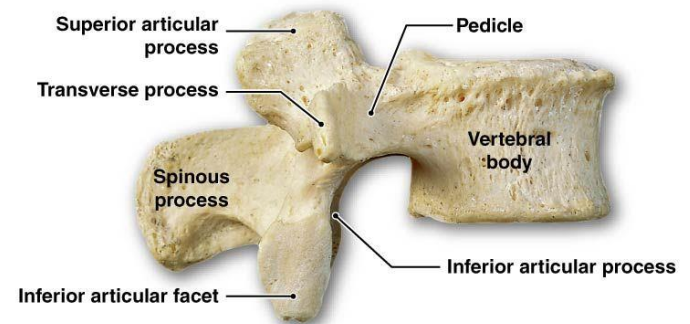
**c** Thoracic vertebra, lateral view.

# LUMBAR VERTEBRAE

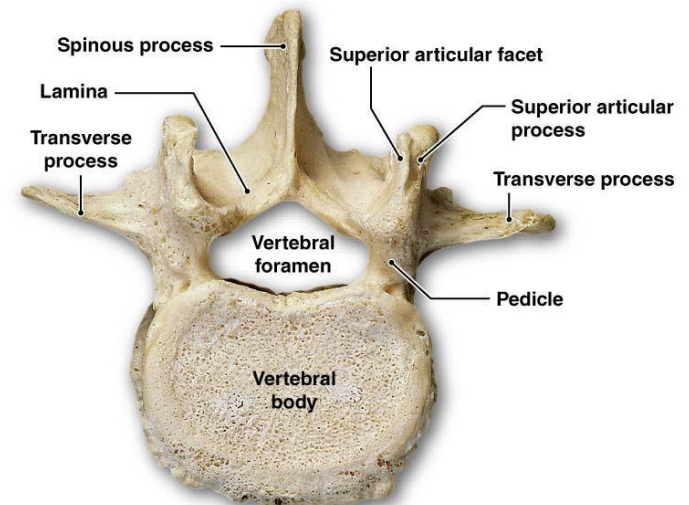
- Typical vertebra: L1-L4
- Atypical vertebra: L5



**a** A lateral view of the lumbar vertebrae, sacrum, and coccyx



**b** A lateral view of a typical lumbar vertebra

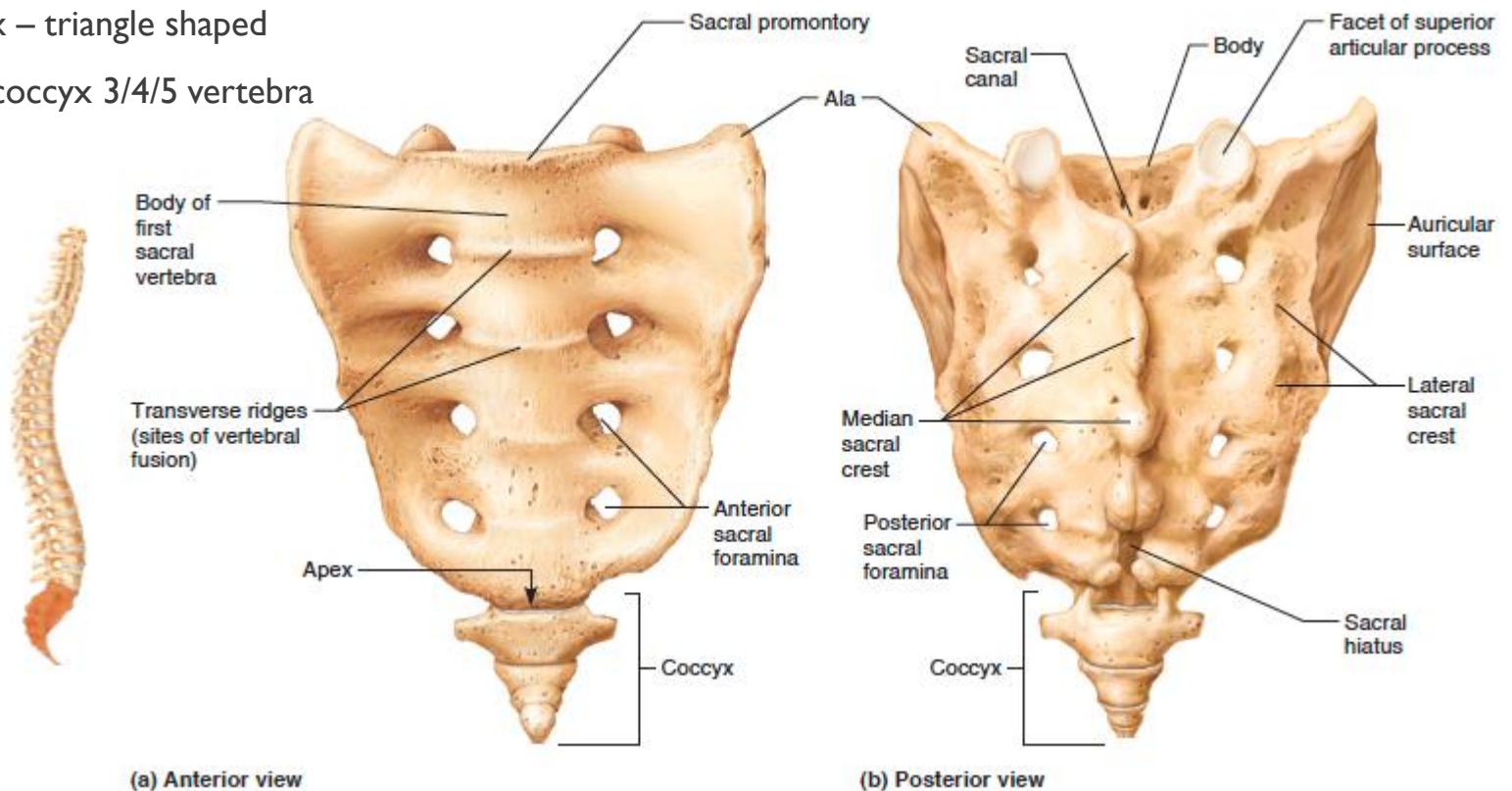


**c** A superior view of the same vertebra shown in part b

# SACRUM AND COCCYX

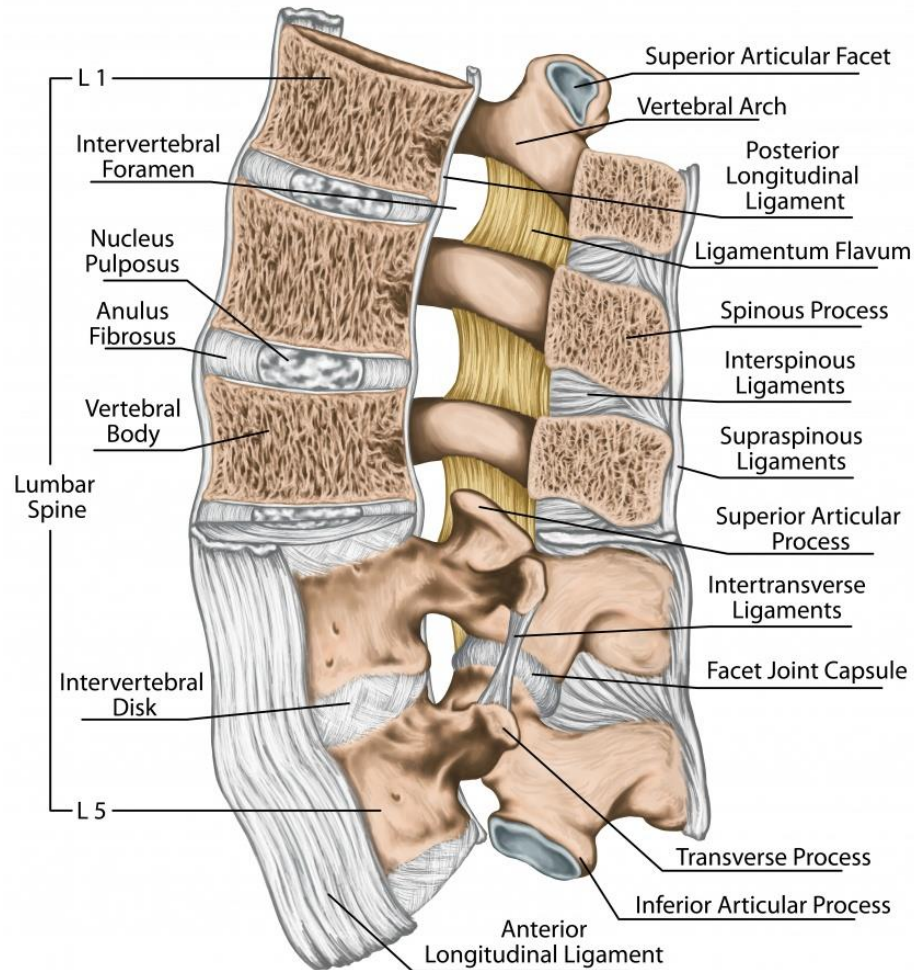


- Sacrum – triangular shaped
- Fused – 5 vertebra
- Coccyx – triangle shaped
- Fused coccyx 3/4/5 vertebra

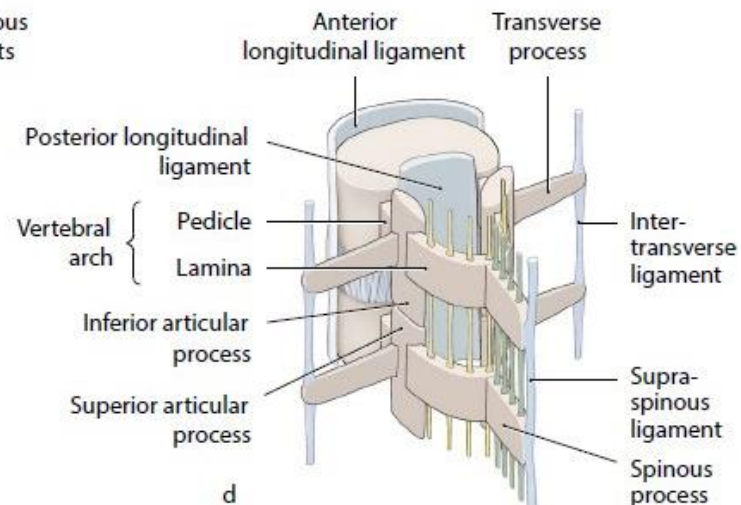
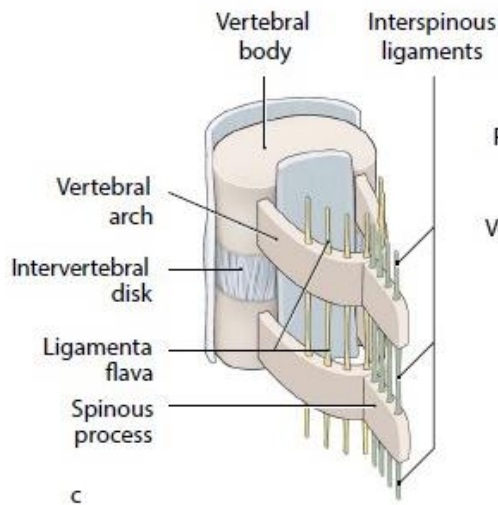
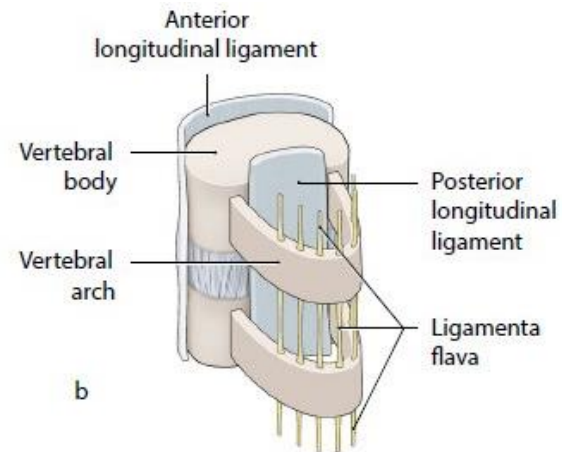
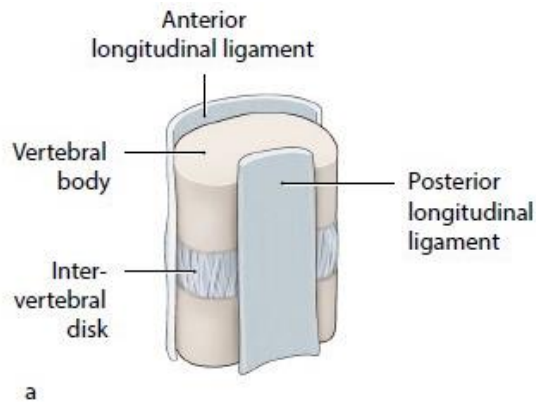




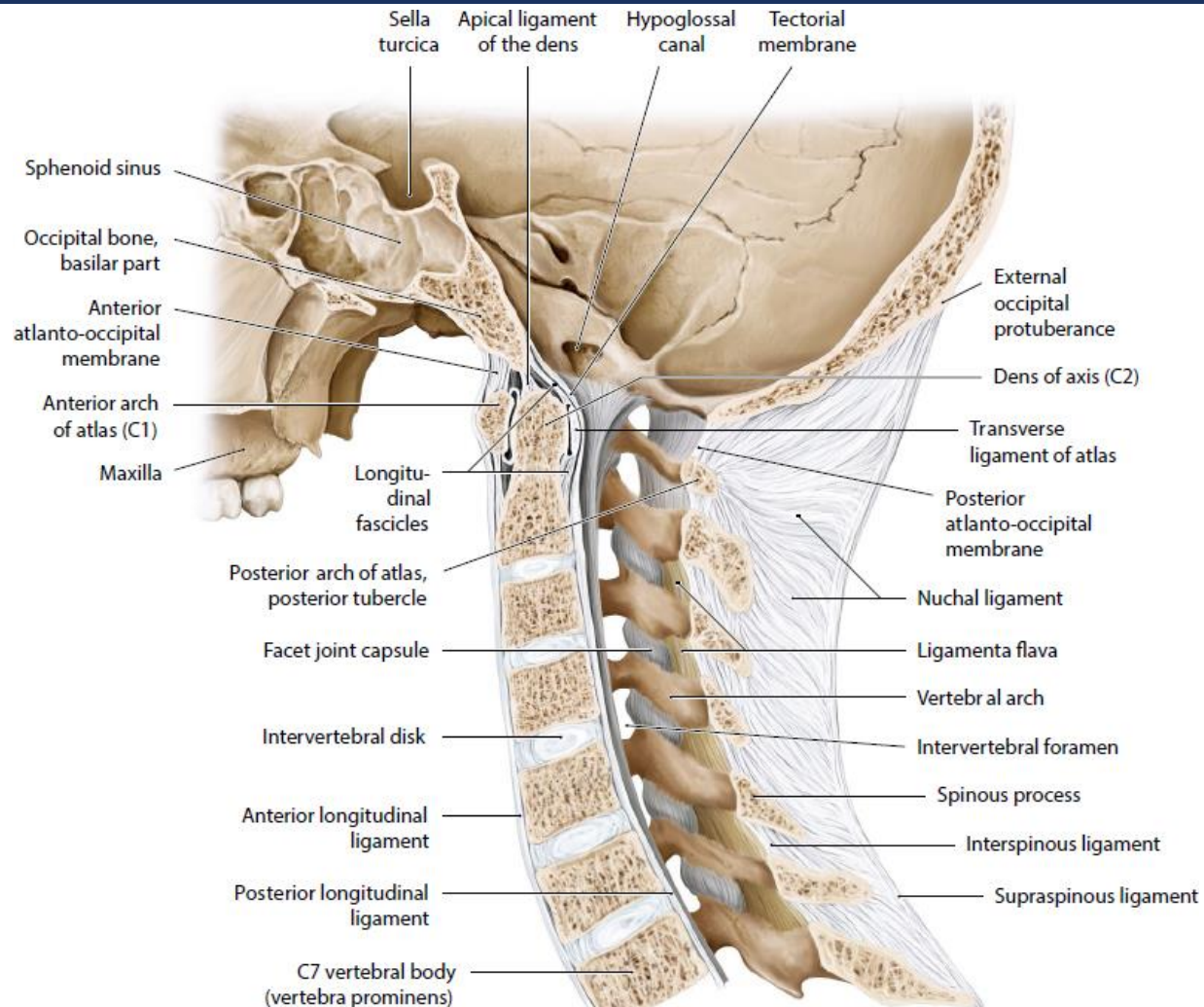
# LIGAMENTS OF THE SPINE



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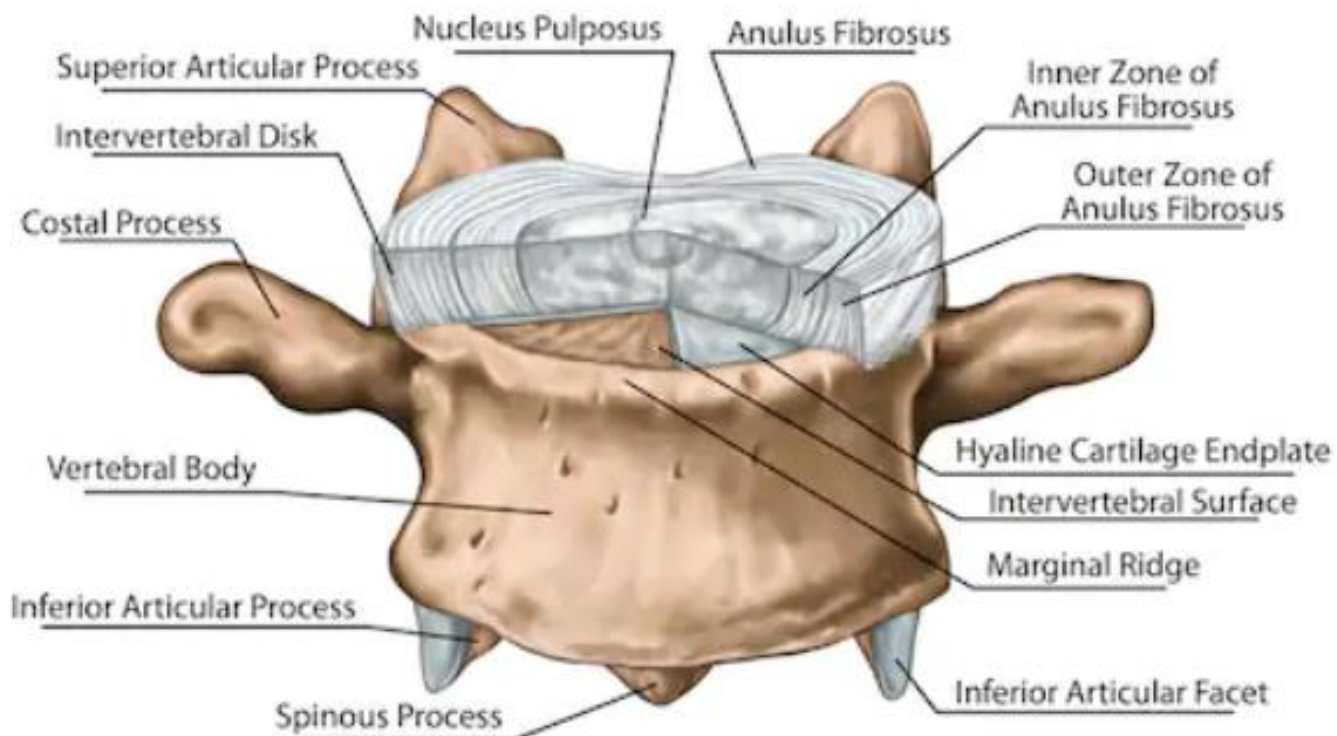


# LIGAMENTS OF THE SPINE



- Give strength to spinal column
- Keep vertebrae in alignment
- Keep discs in position
- Can become damaged through over stretching
- Have a poor blood supply, and therefore a slow recovery from damage

# INTERVERTEBRAL DISKS



# INTERVERTEBRAL DISCS



- Occur between each vertebra and are made up of an annulus and a nucleus.
- Act as separator and shock absorber.
- Pressure within discs can be kept low by maintaining natural curves of the spine and frequent postural changes.
- A healthy back needs all components of the spine to be in good working order



# MUSCLES



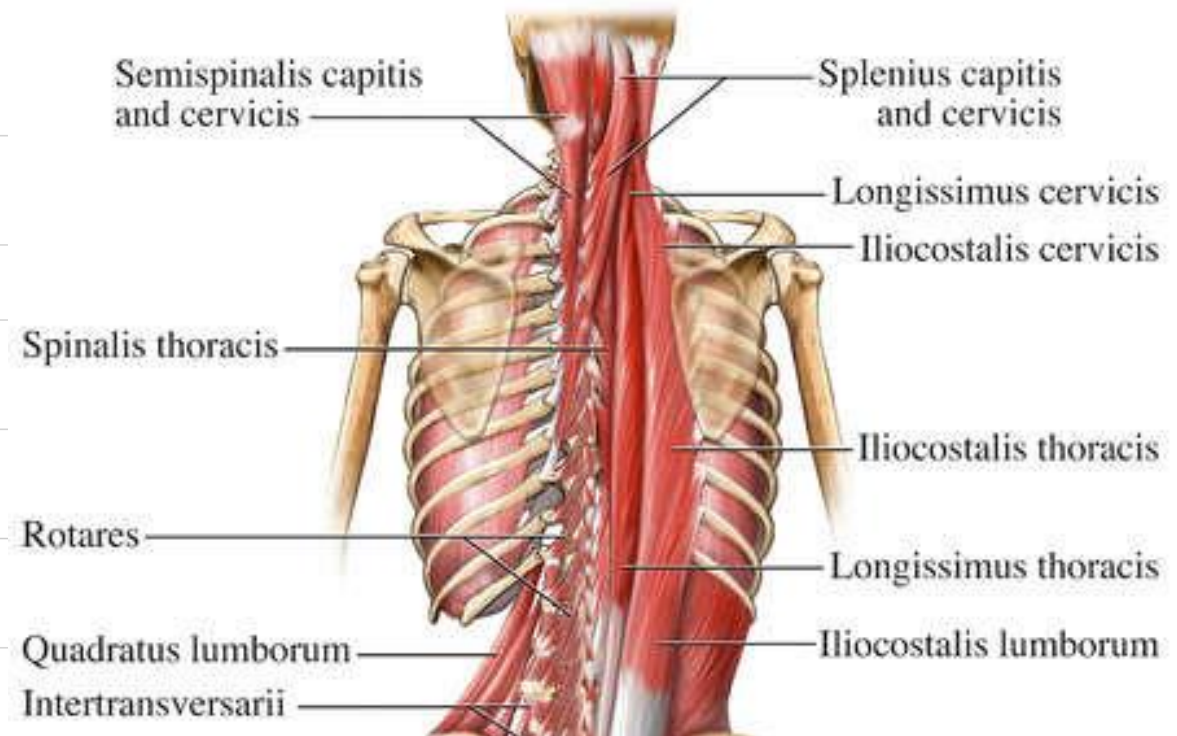
- Work in pairs to maintain postural control.
- Abdominal muscles are important in reducing the stress of lifting.
- Muscle strength and balance
- They are important in maintaining a healthy back.

# LUMBAR MUSCLES



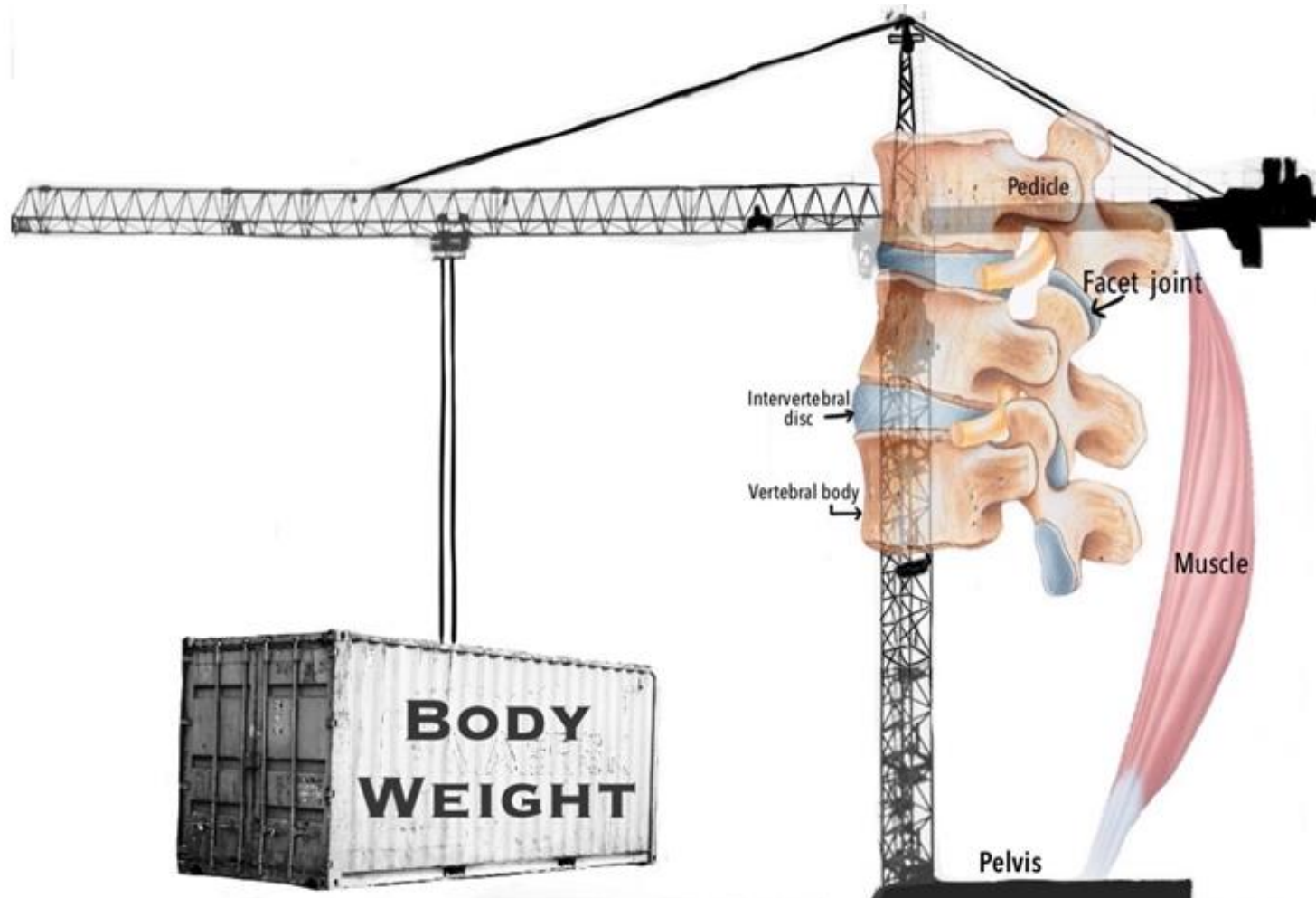
## LUMBAR MUSCLES    FUNCTION

Psoas Major	Flexes thigh at hip joint & vertebral column
Intertransversarii Lateralis	Lateral flexion of vertebral column
Quadratus Lumborum	Lateral flexion of vertebral column
Interspinales	Extends vertebral column
Intertransversarii Mediales	Lateral flexion of vertebral column
Multifidus	Extends & rotates vertebral column
Longissimus Lumborum	Extends & rotates vertebral column
Iliocostalis Lumborum	Extension, lateral flexion of vertebral column, rib rotation





# THE SPINE WORKS LIKE A CRANE



# DISC PRESSURE RELATED TO POSTURE AND MUSCULATURE

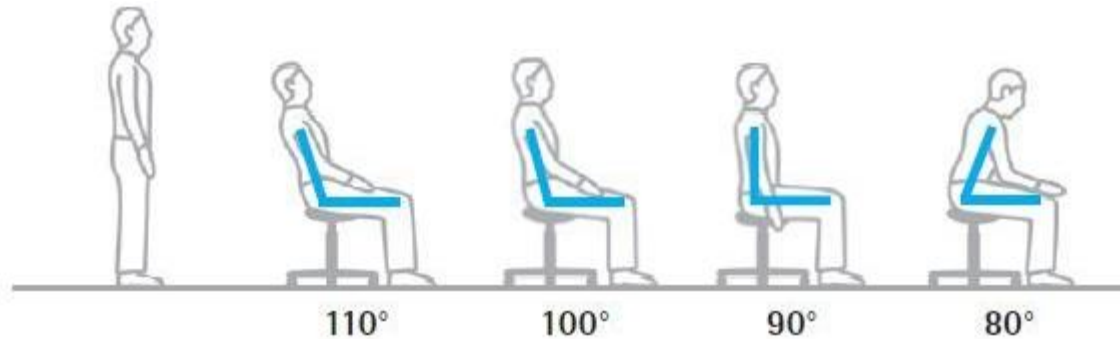


- The weight of your body acts as a compressive and shear forces that in younger people, the intervertebral discs bear most of this load.
- After the discs degenerate, more pressure is transferred to the facet joints in the back, causing arthritis in these synovial joints.
- Cervical Disc Pressure:
  - Correct alignment & muscular support = 5.6kg/cm<sup>2</sup>
  - Incorrect alignment without correct muscular support = 40kg/cm<sup>2</sup>

# HOW POSTURE AFFECTS DISC PRESSURE

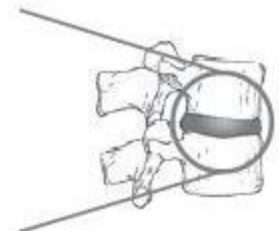
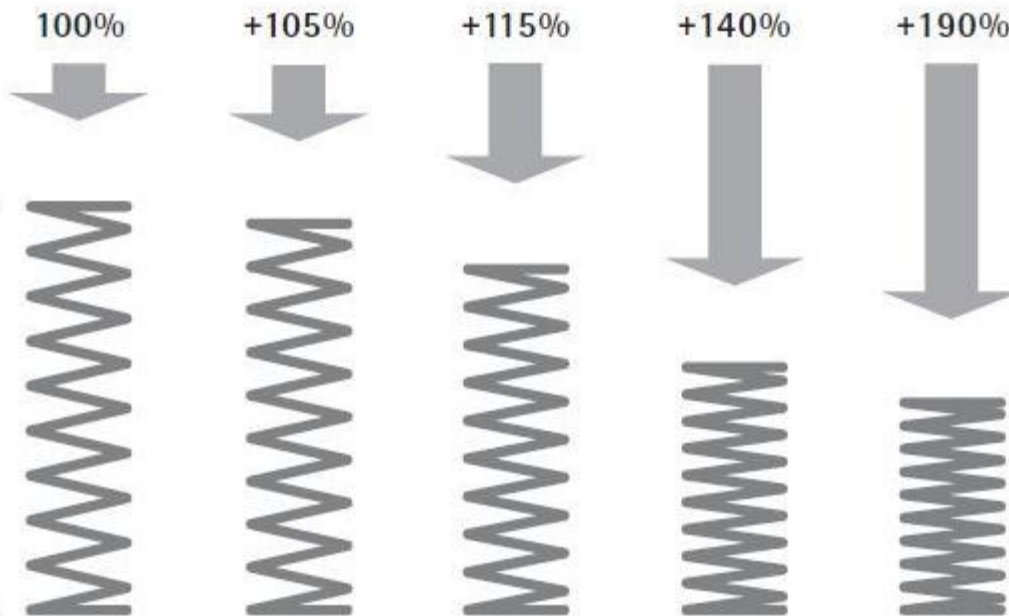


Back angle



Disc pressure

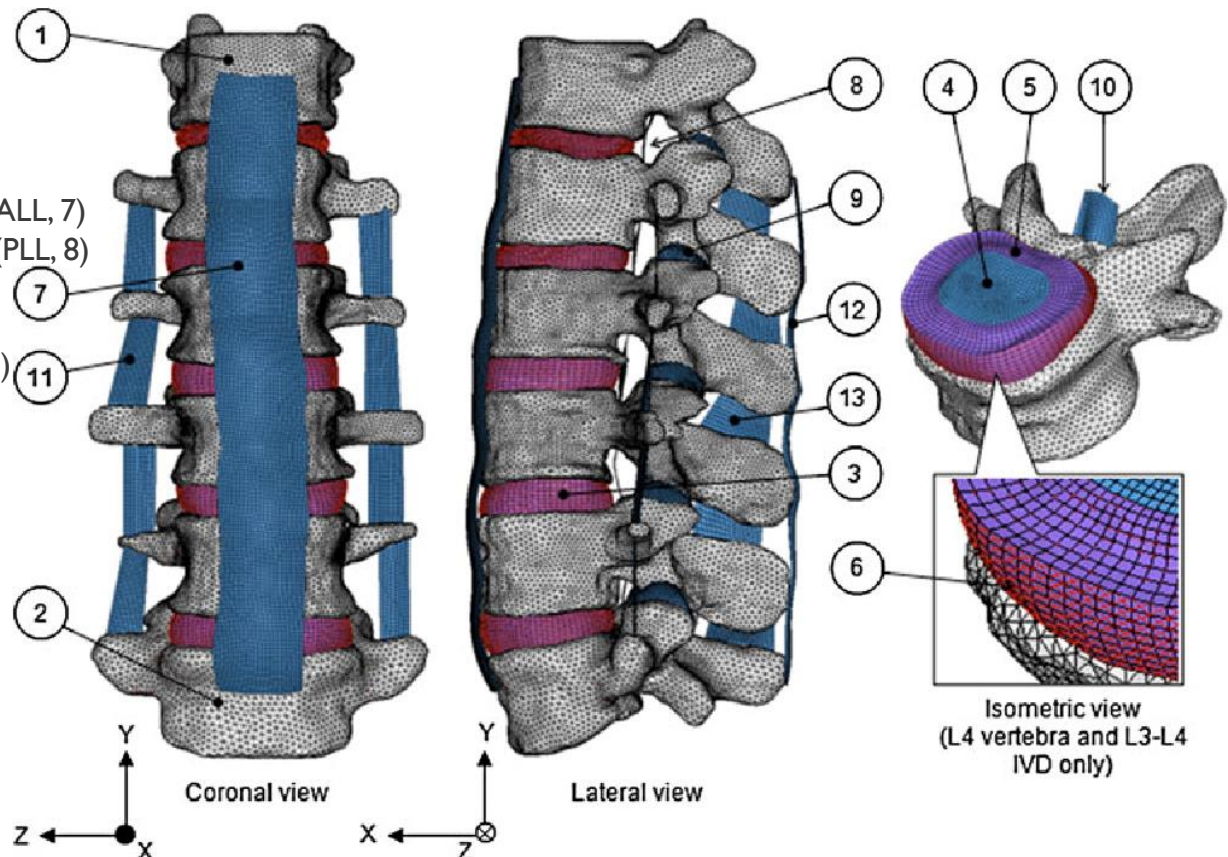
The effect of four postures on the intervertebral disc pressure as measured between the 3rd & 4th lumbar vertebrae. The pressure when standing is taken as 100%.  
According to Nachemson and Elfstrom.



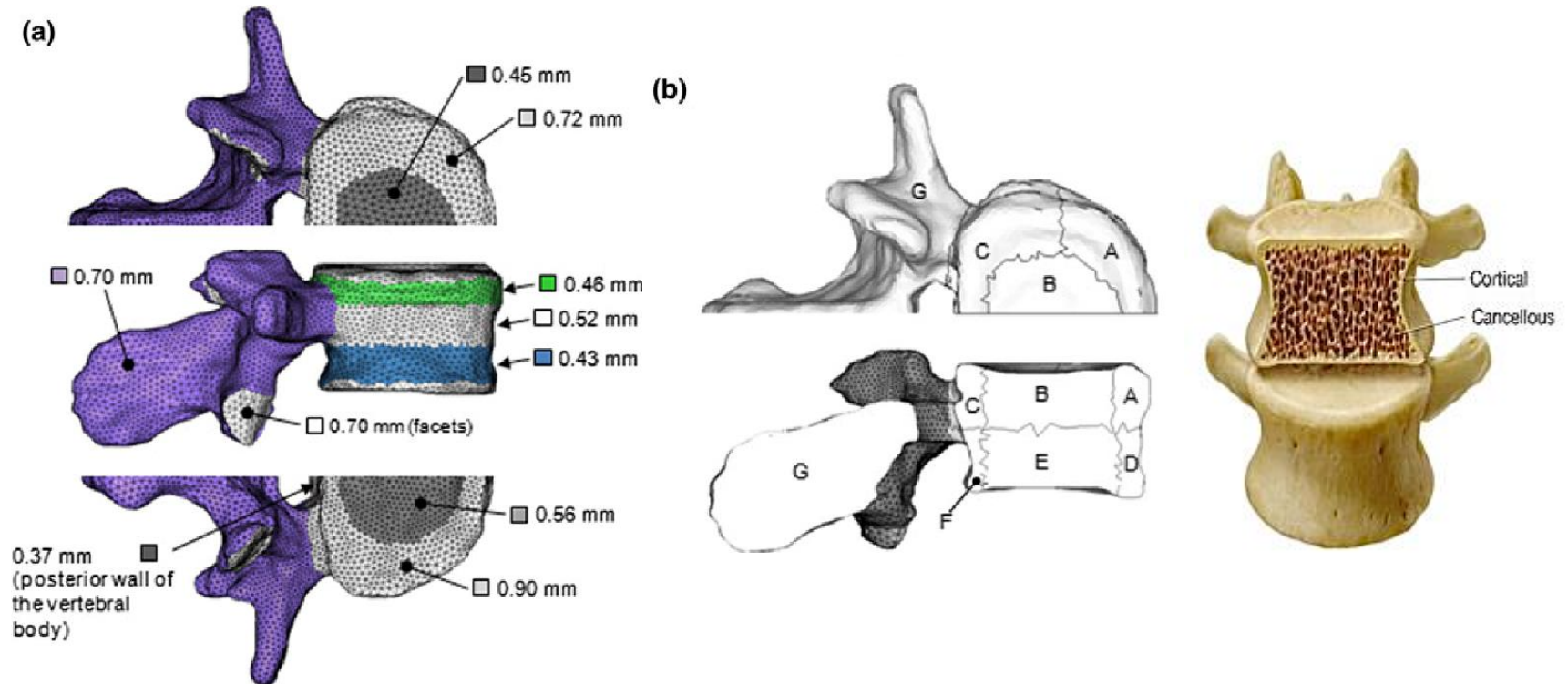
# FINITE ELEMENT MODEL OF T12-L5 SEGMENT OF THE SPINE



- T12 (1) to L5 (2) vertebrae
- Intervertebral discs (3)
- Nucleus (4)
- Annulus (5)
- Collagen fibers (6)
- Anterior Longitudinal Ligament (ALL, 7)
- Posterior Longitudinal Ligament (PLL, 8)
- Capsular Ligament (CL, 9)
- Flavum Ligament (FL, 10)
- Intertransverse Ligament (ITL, 11)
- Supraspinous Ligament (SSL, 12)
- Interspinous Ligament (ISL, 13)



# CORTICAL AND CANCELLOUS BONES



(a) Subdivision of the vertebrae into nine zones of different cortical bone thicknesses

(b) Subdivision of the cancellous bone into seven zones of different material properties

# MECHANICAL PROPERTIES OF BONY TISSUES



Material properties	Cancellous bone (per zone) and bony endplate center <sup>a</sup>							Cortical bone and bony endplate margin
	A	B	C	D	E	F	G	
Density ( $\times 10^{-3}$ g/mm <sup>3</sup> )	1.8	1.8	2.0	2.0	2.5	2.5	1.8	0.2
Modulus of elasticity, $E$ (MPa)	93.7	93.7	93.7	93.7	93.7	93.7	93.7	4,014
Poisson's ratio, $\nu$	0.25	0.25	0.25	0.25	0.25	0.25	0.25	0.3
Yield stress, $a$ (MPa)	1.95	1.95	1.95	1.95	1.95	1.95	1.95	105
Hardening modulus, $b$ (MPa)	8.5	7.0	8.5	8.1	12.5	12.5	7.0	492.9
Hardening exponent, $n$	1	1	1	1	1	1	1	1
Failure plastic strain, $\varepsilon_p$	0.082	0.06	0.082	0.08	0.104	0.104	0.06	0.071
Maximum stress (MPa)	2.65	2.3	2.65	2.6	3.25	3.25	2.3	140
Strain rate coefficient, $c$	0.533	0.533	0.533	0.533	0.533	0.533	0.533	0.272
Reference strain rate, $\dot{\varepsilon}_0$	0.008	0.008	0.008	0.008	0.008	0.008	0.008	0.008

<sup>a</sup> Material properties used for the bony endplate center are the same as zone B

Wagnac, E., Arnoux, P. J., Garo, A., & Aubin, C. E. (2012). Finite element analysis of the influence of loading rate on a model of the full lumbar spine under dynamic loading conditions. *Medical & biological engineering & computing*, 50(9), 903-915.

# MECHANICAL PROPERTIES OF THE SOFT TISSUES



	Material properties	Nucleus pulposus		Annulus matrix		Fibers		
		Low dyn.	High dyn.	Low dyn.	High dyn.			
Intervertebral Discs	a.							
	Density ( $E^{-6} \text{ kg/mm}^3$ )	1	1	1.2	1.2	–		
	Poisson's ratio, $\nu$	0.499	0.499	0.45	0.45	–		
	$C_{10}$	0.64	31.8	0.24	11.8	–		
	$C_{01}$	–0.16	–8.0	–0.06	–2.9	–		
	Load–disp. curve	–	–	–	–	Nonlinear		
	Material properties	Spinal ligaments						
		ALL	PLL	CL	LF	ISL	SSL	ITL
Spinal Ligaments	b.							
	Density ( $E^{-6} \text{ kg/mm}^3$ )	1	1	1	1	1	1	1
	Modulus of elasticity $E$ (MPa)	19.2	84.1	0.6	4.2	4.7	10.2	4.7
	Poisson's ratio, $\nu$	0.4	0.4	0.4	0.4	0.4	0.4	0.4
	Update coef., $E_1$ (MPa/ms)	469.4	1,432.1	3.6	199.7	98.3	476.5	98.3
	Update coef., $E_2$ (MPa)	19.0	83.5	0.6	4.0	4.6	10.0	4.6
	Failure strain, $\varepsilon_1$	0.68	0.38	1.75	1.01	1.10	0.94	1.10
	Failure strain, $\varepsilon_2$	0.90	0.50	1.85	1.25	1.30	1.08	1.30
Scaling function, SF	Tabulated curves							

Wagnac, E., Arnoux, P. J., Garo, A., & Aubin, C. E. (2012). Finite element analysis of the influence of loading rate on a model of the full lumbar spine under dynamic loading conditions. *Medical & biological engineering & computing*, 50(9), 903-915.

# MECHANICAL PROPERTIES OF THE THORACOLUMBAR-PELVIS COMPLEX



Component	Young's Modulus (MPa)	Poisson's Ratio	Density (kg/mm <sup>2</sup> )	Cross-Section Area (mm <sup>2</sup> )
Cortical bone	14,000	0.30	1.83E-06	
Cancellous bone	100	0.2	0.17E-06	
Posterior elements	3,500	0.25	1.83E-06	
Endplate	10,000	0.25	1.06E-06	
Pelvis	5,000	0.2	1.83E-06	
Annulus	Mooney–Rivlin $c = 0.18$ , $c = 0.045$		1.0E-06	
Nucleus pulposus	Mooney–Rivlin $c1 = 0.12$ , $c2 = 0.03$		1.2E-06	
Collagenous fiber	Calibrated stress-strain curves			
Ligament				
ALL	Calibrated deflection-force curves		1.0E-06	63.7
PLL	Calibrated force-deflection curves		1.0E-06	20
FL			1.0E-06	40
ITL			1.0E-06	3.6
ISL			1.0E-06	40
SSL			1.0E-06	30
CL			1.0E-06	60

*Note:* ALL, anterior longitudinal ligament; PLL, posterior longitudinal ligament; FL, ligamentum flavum; ITL, intertransverse ligament; ISL, interspinous ligament; SSL, supraspinous ligament; CL, capsular ligament.